NMR of glycogen in exercise

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Natural-abundance ¹³C NMR spectroscopy is a non-invasive technique that enables *in vivo* assessments of muscle and/or liver glycogen concentrations. Over the last several years, ¹³C NMR has been developed and used to obtain information about human glycogen metabolism with diet and exercise. Since NMR is non-invasive, more data points are available over a specified time course, dramatically improving the time resolution. This improved time resolution has enabled the documentation of subtleties of muscle glycogen re-synthesis following severe glycogen depletion that were not previously observed. Muscle and liver glycogen concentrations have been tracked in several different human populations under conditions that include: (1) muscle glycogen recovery from intense localized exercise with normal insulin and with insulin suppressed; (2) muscle glycogen recovery in an insulin-resistant population; (3) muscle glycogen depletion during prolonged low-intensity exercise; (4) effect of a mixed meal on postprandial muscle and liver glycogen synthesis. The present review focuses on basic ¹³C NMR and gives results from selected studies.

Muscle metabolism: NMR: Glycogen: Exercise: Insulin

With the development of human ¹³C NMR it is now possible to measure glycogen concentrations in individual muscles without resorting to traditional invasive techniques. The musculature has long been an organ of intense interest in the exercise science community. During exercise muscle glycogen levels are reduced according to the type of exercise, and reflect variables such as workload and rate of contraction (Ivy et al. 1987; Price et al. 1991, 1994a; Robergs et al. 1991). Intense exercise can deplete the bulk of glycogen in a muscle in as little as 10 min (Price et al. 1994a). When exercise ceases, the exercised muscles then resynthesize glycogen at a rate that is influenced by the concentration of glycogen remaining within the muscle (Price et al. 1994a). ¹³C NMR provides non-invasive and continuous assessment of muscle glycogen concentrations and their dependence on diet and exercise.

Until recently, information about the complicated patterns of muscle glycogen balance and its relationship with exercise has only been available by using needle biopsies that could measure muscle glycogen concentrations (Harris *et al.* 1974; Dietrichson *et al.* 1987). While biopsies provided the original broad outline of muscle glycogen metabolism, the number and frequency of measurements and the sampling of only a small volume in a non-

homogeneous tissue were limitations of the method (Taylor *et al.* 1992). With the advent of *in vivo* natural-abundance ¹³C NMR it has become possible to obtain glycogen measurements non-invasively following depletion, with better time resolution, repeatability, and somewhat better precision (Taylor *et al.* 1992; Price *et al.* 1994*a*). Using ¹³C NMR an extremely rapid separate phase of glycogen resynthesis was distinguished from the slower subsequent resynthesis. (Price *et al.* 1994*a*). Although the qualitative features of an initial rapid rate of resynthesis that was not insulin sensitive, followed by a slower insulin-dependent synthesis had been outlined by biopsy measurements (Maehlum *et al.* 1977), the quantitative separation of the rates into two periods, as shown by the ¹³C NMR, provided a more distinct interpretation.

However, ¹³C NMR is not without its drawbacks, that include the availability of expensive well-maintained equipment, and the inability to distinguish between fibre types (Taylor *et al.* 1992). When performed in natural abundance, signal : noise becomes an issue with ¹³C NMR. Several hundred dollars-worth of enriched glucose can increase ¹³C NMR signal by one order of magnitude above natural abundance in a normal human study. In addition, these NMR methods are confined to measuring the

Abbreviations: G6P, glucose-6-phosphate; NIDDM, non-insulin-dependent diabetes mellitus; RF, radiofrequency. *Corresponding author: Dr Thomas B. Price, fax +1 203 785 6534, email price@boreas.med.yale.edu

concentration of muscle metabolites including glycogen (Avison *et al.* 1988), glucose-6-phosphate (G6P; Rothman *et al.* 1992), creatine phosphate, inorganic phosphate (Gadian *et al.* 1979) and lactate (Pan *et al.* 1989), while enzymic rates must be calculated from changing concentrations in label. The complementary abilities of NMR and biopsy methods create opportunities to combine the techniques, and to gain a deeper understanding of muscle metabolism during exercise and recovery.

A question often asked about the ¹³C NMR measurement of glycogen is why it is performed at only a small number of laboratories. The primary limitation in making the measurement more widespread is that most standard magnetic resonance imaging and spectroscopy systems are unable to perform the glycogen measurement without hardware and software modifications. Although it is beyond the scope of the present review to describe this equipment in detail, we provide a short list here of the additional equipment required. The ¹³C NMR glycogen resonance is detected by measuring the induced voltage in a radiofrequency (RF) coil from the time-varying magnetic field emitted by the glycogen ¹³C nuclei. The resonance frequency depends both on the nucleus and the chemical environment of the nucleus. A standard clinical magnetic resonance system is unable to receive the glycogen RF signal because it is tuned only to receive the frequency of the ¹H nuclei in water. In order to convert a magnetic resonance imaging system to be able to measure glycogen. an additional receiver channel is required tuned to the ¹³C frequency, including an RF coil tuned to the ¹³C nuclei. A further complication is that, due to interactions with bound ¹H nuclei, the resonance of $[1-^{13}C]$ glycogen is split into two frequencies, which complicates detection. To eliminate this interaction, referred to as J-coupling, it is necessary to apply energy at the resonance frequency of the bound glycogen ¹H nuclei (decoupling) during the acquisition of the ¹³C signal. This energy must be applied with a separate RF coil tuned to the ¹H frequency. Furthermore, an additional RF amplifier and RF frequency generator is required to produce the RF energy transmitted from the decoupling coil. The energy applied at the ¹H frequency will introduce noise into the ¹³C receiver unless care is taken with appropriate RF filters to block the energy from reaching the ¹³C receiver. Once the appropriate hardware and software is available the primary limitations on the accuracy of the NMR measurement are sensitivity, and calibration against an external glycogen standard. Calibration of the glycogen measurement requires that the signal obtained from the muscle be compared with the signal obtained from a solution of glycogen that encompasses the same volume as the muscle. If the muscle is smaller than the receiving field of the ¹³C RF coil, it may be difficult to make an accurately-shaped standard. An alternative is to use localized spectroscopy which selects a volume defined independently of the receiving field of the coil (Rothman et al. 1990). The disadvantage of using localization is that the programming of the system to perform these experiments is more complicated.

Methods of ¹³C NMR acquisition and data processing have been described in detail in a number of publications (Avison *et al.* 1988; Jue *et al.* 1989; Price *et al.* 1991, 1994*a*; Taylor *et al.* 1992, 1993, 1996). Briefly, in order to obtain a

¹³C NMR spectrum a simple proton decoupled pulseacquire pulse programme is used. A surface coil RF probe is positioned at the skin surface adjacent to the specific muscle of interest. Information about glycogen is obtained from the spectral resonance that corresponds to the 1-¹³C of glucose in the glycogen-bound form. The integral area beneath this resonance is a direct indication of the number of 1-13C of glucose present in the glycogen-bound form. Chemical concentrations of glycogen are determined by comparing each human in vivo spectrum with a spectrum obtained from an external standard solution of known glycogen concentration (150-200 mmol/l). These values agree well with the values obtained by direct biochemical assay of muscle samples obtained from the same human subject and on the same day (Taylor et al. 1992). In these studies, uniform positioning of the probe and the subject was verified with magnetic resonance imaging, and ¹³C NMR signals were obtained in natural abundance, which is only 1.1%. When necessary, the ${}^{13}C$ signal strength can be increased by totally 1-13C-enriched glucose, which will increase the ¹³C signal by a factor of approximately 100. Even increasing the $1-^{13}C$ signal by a factor of 10 extends the sensitivity significantly at a modest cost.

The quantifiable visibility of glycogen was established by Sillerud & Shulman (1983) when ¹³C NMR spectra of glycogen in solution gave sharp resonances from approximately 100% of the C nuclei. A subsequent study demonstrated that these resonances were also visible in the perfused rat liver (Shulman et al. 1988). Proof of the visibility has been necessary because a macromolecule the size of glycogen would not give sharp visible lines if it were rigid. In subsequent NMR studies it was demonstrated that the large glycogen molecules had extensive internal motion (Zang et al. 1990a,b). A subsequent study demonstrated that muscle glycogen was 100% visible in a skinned rabbit muscle preparation (Gruetter et al. 1991). In a human population, an NMR validation study focused on repetitive 5 min measurements of the same muscle to evaluate reproducibility (Taylor et al. 1992). The study reported a CV that was 4.3%, which for the basal muscle glycogen level of approximately 80 mmol/l was ± 3.4 mmol/l (Tavlor et al. 1992). As expected, the accuracy of these measurements depended on the NMR signal:noise value, which improved as the square root of the time of measurement. Several measurements with 20 min of acquisition have yielded the expected twofold smaller CV (Price et al. 1991). However, the validation study had shown that even 5 min data acquisitions possessed an accuracy that was significantly better than that reported from biopsy measurements (Taylor et al. 1992). During these experiments it became clear that the errors were due to the signal:noise value of the NMR spectra, and that no additional uncertainties were introduced when the subjects left the magnet between measurements. Since optimum data acquisition conditions of magnet shimming and probe tuning could be reached within several minutes, there were no serious disadvantages in allowing the subject to leave the magnet between data acquisitions. As suitable NMR equipment has become available, well-resolved ¹³C resonances have been regularly observed in vivo in both animal and human muscle and liver (Shulman et al. 1990; Price et al. 1994a; Taylor et al. 1996).

Exercise studies of muscle metabolism

The initial application of ¹³C NMR to human exercise studies was a measurement of glycogen levels in the gastrocnemius muscles of two athletic males before and after they ran a half-marathon (Avison et al. 1988). These results showed a 70% decrease in the muscle glycogen concentration and the depleted muscle glycogen returned to 80% of baseline during the next 19h (Fig. 1). While the initial exercise experiment employed an exercise protocol (Avison et al. 1988) that resulted in substantial changes in systemic variables (e.g. blood glucose, lactate and pH), subsequent studies have employed a localized-exercise protocol (Price et al. 1991, 1994a,b). Localized exercise buffers the systemic response for the study of glycogen metabolism by NMR. The results obtained from localized muscle measurements are consistent with the idea that during a localized-exercise protocol glycogen synthesis in the exercised muscle is under local control. The pathways of glucose uptake and glycogen metabolism are pictured schematically in Fig. 2. Glucose transported into the muscle that is increased as the result of exercise or insulin stimulation is phosphorylated by hexokinase (EC 2.7.1.1) to G6P and then incorporated into muscle glycogen (via two intermediates) or used directly by the muscle to generate energy via glycolysis.

In early studies muscle glycogen change was examined with localized low-intensity exercise of the gastrocnemius muscle (workloads of 15–25% maximum voluntary contraction for the gastrocnemius muscle; Price *et al.* 1991, 1994*b*). Previous biopsy studies had reported that during exercise of low-to-moderate intensity (Costill *et al.* 1973) an initial period of glycogen depletion is followed by a period of constant glycogen levels despite continued exercise. In localized plantar flexion exercise (15–25% maximum voluntary contraction) gastrocnemius glycogen declined for $2 \cdot 5$ (SE $0 \cdot 5$) h and then exhibited no further net decrease during $5 \cdot 5$ h of continued exercise (Price *et al.* 1991). This observation suggested an increased contribution from alternative C sources such as blood glucose or free fatty acids.



Fig. 1. The variation of intensity of the [1-¹³C]glycogen doublet (undecoupled spectrum) in response to exercise. Spectrum A was collected from the gastrocnemius muscle of a trained runner 1 h before a 13 mile run. Spectrum B was collected from the same location immediately after the run. Spectrum C was collected the following morning (19 h after the run). These spectra, collected before natural-abundance ¹³C NMR spectra were routinely decoupled, were presented in the initial report on the utility of NMR to detect exercise-induced changes in muscle glycogen. (From Avison *et al.* 1988; with permission.)

Although the net glycogen consumption ceased during this level period, the question remained as to whether the rates of glycogen synthesis and degradation both go to zero or whether these two pathways continue to be active resulting in turnover of the C in the muscle glycogen pool. This kind of turnover is known to occur in rat muscle and liver (Shulman et al. 1988; Hutber & Bonen, 1989; David et al. 1990) and also in human (Magnusson et al. 1991, 1995) liver. However, there was no evidence that this energyexpensive process operates in individual human skeletal muscles. The plateau period of no net glycogen depletion could have resulted from cessation of glycogen depletion or from a dynamic steady-state in which glycogen synthesis and degradation rates matched one another. A subsequent study was performed in which 1-13C-labelled glucose was infused in order to increase the signal from glucose incorporation into glycogen and thus allow turnover of muscle glycogen to be detected during the plateau period (Price et al. 1994b). The results of that study indicated that there was turnover of glycogen within an individual muscle that was exercised for a prolonged period at a constant workload, and that turnover occurred during the previously-established plateau period of constant glycogen concentration (Costill et al. 1973; Constable et al. 1984; Price et al. 1991). In this localized-exercise protocol, infused [1-13C] glucose was incorporated into exercising muscle glycogen, but not into non-exercising muscle glycogen, during the infusion period. However, because the subjects stopped exercising while the ¹³C NMR measurement was made, some uncertainty exists as to whether the glycogenesis occurred during the exercise or during the measurement. These experiments are currently being repeated with the NMR spectra acquired during exercise.

The methods employed in these localized-exercise and NMR studies consider the muscle as a whole and do not directly address the possibility that synthesis and degradation occur in different muscle fibres. Previous studies using exercise of large muscle groups had observed that at low-intensity workloads (<45% maximum O₂ uptake) glycogen depletion in slow-twitch fibres preceded depletion in fast-twitch fibres (Gollnick et al. 1974; Vollestad & Blom, 1985). Gollnick et al. (1974) demonstrated that after 3 h of pedalling exercise at 31 % maximum O₂ uptake almost all the 50% of muscle glycogen remaining in the human quadriceps femoris was in fast-twitch fibres. When 60% of the glycogen in that muscle remained (2h exercise) there was a significant amount present in slowtwitch fibres, although all slow-twitch fibres were partially depleted (Gollnick et al. 1974). Conversely, Ivy et al. (1987) reported that when the workload was moderate, all muscle fibres shared in contraction. Hence, the assessment of workload is of primary importance in understanding the results of this type of study.

More recent studies have examined the effect of an intense glycogen-depleting exercise protocol (50%) maximum voluntary contraction) on the period of recovery immediately following cessation of exercise. In the initial study of this series three exercise protocols (standing single-leg toe-raises) of different durations were performed, with intensities determined by the body weight of each subject (Price *et al.* 1994*a*). To reduce lactate accumulation in the



Fig. 2. Biochemical schematic of muscle and liver glycogen/glucose metabolism. Either insulin or exercise, or a combination of the two, may induce glucose transport via glucose transporter 4 (GLUT4) into muscle. Intramuscular glucose is then phosphorylated by hexokinase (*EC* 2.7.1.1; HK) into glucose-6-phosphate (G6P), and thereafter incorporated by glycogen synthase (*EC* 2.4.1.11; GS) into muscle glycogen. GP, glycogen phosphorylase (*EC* 2.4.1.1); TCA, tricarboxylic-acid cycle; G6Pase, glucose-6-phosphatase (*EC* 3.1.3.9).

muscle during exercise, subjects alternated toe-raises for 1 min (approximately thirty-five rises per min) with rest for 1 min throughout the exercise period. During exercise subjects maintained full extension of their knee in order to isolate the work. Based on assessment of maximal voluntary contraction, the mean workload was 51 (SE 5) % maximum voluntary contraction (39–67%). The exercise durations depleted glycogen in the gastrocnemius to approximately

75, 50 or 25 % resting levels (11.3 (SE 1.8), 14.6 (SE 1.2), 26.1 (SE 3.5) min respectively; mean glycogen depletion rate 196 (SE 17) mmol/1 per h) assessed by natural abundance ¹³C NMR spectroscopy (Price *et al.* 1994*a*). Plantar flexion exercise was performed from an erect standing position (single-leg toe raises) in order to selectively exercise the gastrocnemius. Total work values (kJ) were 22.1 (SE 4.9), 31.3 (SE 3.4), and 45.3 (SE 6.5) kJ respectively for depletion to 75, 50 and 25% resting glycogen concentrations. The human gastrocnemius muscle is made up of approximately 60 % slow-twitch (oxidative) fibres and approximately 40 % fast-twitch (glycolytic) fibres. Although these fibre types are differentially recruited at light-to-moderate workloads, heavy exercise is known to deplete glycogen in all fibres (Ivy et al. 1987). Thus, it was assumed that the heavy load placed on the gastrocnemius in this exercise protocol recruited all fibres within the muscle (Ivy et al. 1987).

This localized-exercise protocol was used to study the effects of glycogen depletion and insulin concentration on glycogen synthesis. Gastrocnemius glycogen was measured with ¹³C NMR before exercise and for 5 h following exercise. Subjects performed single-leg toe raises to deplete gastrocnemius glycogen to 75, 50 or 25 % resting concentration. After depletion to 75 and 50% resting levels, glycogen resynthesis rates were similar (2.4 (SE 0.7) and 2.8 (SE 0.6) mmol/1 per h respectively) as shown in Fig. 3 (Price et al. 1994a). When glycogen was depleted to 25% (<30 mmol/1), the initial resynthesis rate was significantly higher (P < 0.02) at 33 (SE 7) mmol/1 per h, and it declined to 3.5 (SE 0.9) mmol/1 per h at > 35 mmol glycogen/1 (Price et al. 1994a). In the same study, insulin dependence of glycogen synthesis was assessed after depletion to 25 % resting levels with and without infusion of somatostatin to inhibit insulin secretion (Price et al. 1994a). A subset of subjects (n 5) each depleted gastrocnemius glycogen to



Fig. 3. Time-course of gastrocnemius muscle glycogen from depletion to 75 (\bullet), 50 (\blacktriangle) and 25 (\Box) % resting concentration. Values are means with their standard errors represented by vertical bars for three, eight and eight trials at 75, 50 and 25% resting glycogen concentrations respectively. (—), Linear regression analysis. At 25% resting glycogen the linear regression is split into two time periods (0–45 min and 1–6 h) (From Price *et al.* 1994*a*; with permission.)

25% resting levels in a paired study with and without infusion of somatostatin to suppress insulin release. At <35 mmol/1 glycogen synthesis was not significantly affected by low insulin (24 (SE 4) mmol/1 per h with insulin v. 19 (SE 3) mmol/1 per h without insulin), whereas at >35 mmol glycogen/1, synthesis ceased without insulin (3.3 (SE 0.8) mmol/1 per h with insulin v. -0.07 (SE 0.19)mmol/1 per h without insulin (Fig. 4; Price et al. 1994a). The study concluded that after depletion to < 30 mmol/1 perh initial glycogen resynthesis was insulin independent, and concurred with the findings of Garetto et al. (1984) who reported two phases of glycogen recovery in the rat muscle following intense exercise, one of which was insulin dependent. It was also consistent with observations by Maehlum et al. (1977) on subjects with insulin-dependent diabetes mellitus who showed an early glycogen repletion that was independent of insulin. Since ¹³C NMR studies have the advantage that synthesis rates can be measured more accurately over a longer time interval and with considerably better time resolution, the NMR study demonstrated a clear biphasic glycogen recovery pattern in normal human subjects (Price et al. 1994a).

An additional advantage to human in vivo NMR spectroscopy is the ability to study other NMR visible nuclei, particularly ³¹P. In an insulin-glucose clamp, ³¹P NMR was used to determine G6P concentrations in the muscle in vivo (Rothman et al. 1992). Basal concentrations of G6P in the human gastrocnemius muscle were 0.12 (SE 0.01) mmol/1, which was several times lower than those sometimes reported from biopsies (Young et al. 1988; Rosetti & Giaccari, 1990; Rothman et al. 1992). During the hyperinsulinaemic-hyperglycaemic clamp ³¹P NMR measured an increase in G6P concentration in the gastrocnemius muscle. Difference spectra showed wellresolved increases in intensity in the low-field portion of the phosphomonoester regions of the spectrum at positions that were identified as G6P (Fig. 5; Rothman et al. 1992). In an earlier study an increase in spectral intensity was found at the chemical shift characteristic of the ³¹P resonance of G6P



Fig. 4. Paired study of glycogen recovery from depletion to 25% resting concentration under conditions of inhibited insulin (\blacktriangle) with infusion of somatostatin, and under normal insulin conditions (\bigcirc) without somatostatin. Values are means with their standard errors represented by vertical bars for five paired trials. \uparrow , Beginning and end of somatostatin infusion. At 2h into the recovery period, mean glycogen concentrations were significantly lower in the insulin-inhibited group (* $P \le 0.01$). (From Price *et al.* 1994*a*; with permission.)

following human forearm exercise (Pan *et al.* 1989); however, in contrast to the simple increase in the ³¹P spectra seen during the hyperinsulinaemic–hyperglycaemic clamp, the changes in the phosphomonoester region after intense exercise were more complex. With these assignments it was possible to measure the rates of glycogen synthesis (by ¹³C NMR) and the G6P concentrations (by ³¹P NMR) simultaneously in the rat gastrocnemius after intense glycogendepleting exercise (Bloch *et al.* 1994). NMR with its unique ability to examine non-invasively muscle G6P (with ³¹P) and glycogen (with ¹³C) simultaneously with interleaved pulse sequences, was therefore an ideal combination method for assessment of exercise effects on glycogen synthesis in a human population.

Since the initial intense glycogen-depleting exercise study demonstrated that in normal healthy human subjects there was an early phase of rapid glycogen resynthesis (12–30 mmol/l per h) lasting approximately 45 min that was insulin independent and a subsequent period of glycogen resynthesis (above approximately 35 mmol glycogen/l) that was much slower (approximately 3 mmol/l per h) and insulin dependent (Price et al. 1994a), a second exercise study compared control subjects with the insulin-resistant offspring of parents with non-insulin-dependent diabetes mellitus (NIDDM; Price et al. 1996). During the insulinindependent portion of recovery from glycogen-depleting exercise the glycogen recovery rates were not significantly different between the control and the insulin-resistant groups (Fig. 6). However, during the insulin-dependent portion of muscle glycogen resynthesis the control subjects synthesized glycogen at a rate of 2.9 (SE 0.2) mmol/l per h,



Fig. 5. ³¹P NMR spectra of the gastrocnemius muscle of a normal subject. A baseline spectrum and a spectrum acquired over the period of 40–80 min into a low-dose insulin clamp are shown, as well as the difference between these two spectra. In the difference spectrum (clamp minus baseline), an increase during the clamp is observed of the resonances of glucose-6-phosphate (G6P; 7·13 parts per 10⁶ (ppm)) and inorganic phosphate (Pi; 4·88 ppm). The increase is quantitatively accounted for by a decrease in phosphocreatine (PCr; 0·00 ppm), which is not completely shown in the plot owing to its greater resonance amplitude. The increase in the G6P resonance intensity corresponds to a 0·13 mmol/l muscle increase in concentration. (From Rothman *et al.* 1992; with permission.)

while the insulin-resistant subjects showed a negligible rate of muscle glycogen synthesis (0·1 (SE 0·5) mmol/l per h; Fig. 6). This difference in synthesis occurred despite similar plasma concentrations of glucose and higher concentrations of insulin (Price *et al.* 1996). The reduced rate of muscle glycogen synthesis during this period may have been due to an insulin dependent impairment of either glucose transport and subsequent phosphorylation, or glycogen synthase (*EC* 2.4.1. 11). The mean of the G6P data was not significantly different from that for the control subjects, and was similar to pre-exercise values during the insulin-dependent phase. The finding of similar G6P concentration with decreased glycogen synthesis suggests that both glucose transport and subsequent phosphorylation, and glycogen synthase activity are reduced in a coordinated manner.

Exercise and insulin are both known to stimulate muscle glucose uptake and subsequent glycogen synthesis



Fig. 6. Time-courses of (a) glycogen and (b) glucose-6-phosphate (G6P) concentration before, during a single-leg toe-raise exercise protocol (EX), and during 5 h recovery of glycogen-depleted gastrocnemius muscles in age- and weight-matched control (CON; \blacktriangle) and insulin-resistant (IR; O) offspring of parents with adult-onset diabetes mellitus. Values are means with their standard errors represented by vertical bars for eight trials for each group. The insulin-dependent phase of muscle glycogen recovery was significantly impaired in the IR group (* $P \le 0.05$). (From Price *et al.* 1996; with permission.)

in an independent and additive manner (Roch-Norland et al. 1972; Wallberg-Henriksson et al. 1988; Sternlicht et al. 1989; Douen et al. 1990; Goodyear et al. 1990). Under resting conditions the effect of insulin stimulation on glycogen synthesis has been compared in healthy control subjects and in subjects with NIDDM by ¹³C NMR (Shulman et al. 1990). In both control subjects and subjects with NIDDM placed under hyperglycaemichyperinsulinaemic conditions the major pathway of insulindependent glucose metabolism was muscle glycogen synthesis (Shulman et al. 1990). However, in the subjects with NIDDM the rate of muscle glycogen synthesis was significantly slower (Shulman et al. 1990). Fig. 6 demonstrates that following muscle-glycogen-depleting exercise the insulin-resistant offspring of parents with NIDDM had: (1) normal rates of muscle glycogen synthesis and intracellular G6P concentrations during the early insulin-independent phase of recovery from exercise; (2) severely diminished rates of muscle glycogen synthesis during the subsequent recovery period (2-5h) which had been shown to be insulin dependent in normal control subjects (Price et al. 1996). The data provided evidence that exercise and insulin stimulate muscle glycogen synthesis in human subjects by different mechanisms, and that in the insulin-resistant subjects the early response to stimulation by exercise is normal. The results of this study therefore support the existence of distinct mechanisms for exercise and insulin action on the glucose transport step, since normal glucose transport was present in the insulin-resistant subjects following exercise, despite their previously demonstrated impairment of insulin-stimulated glucose transport and subsequent phosphorylation (Shulman et al. 1990).

Muscle and liver glycogen turnover following a mixed meal

A knowledge of carbohydrate storage after a mixed meal is of paramount importance in understanding normal energy metabolism in human subjects. The non-invasive nature of ¹³C NMR has allowed postprandial glycogen storage to be studied in both muscle and liver (Taylor et al. 1993, 1996; Hwang et al. 1995; Petersen et al. 1996). When the combined data of muscle and liver studies are examined, distinct patterns that occur over the first 7 h following a mixed meal can be distinguished. In all studies a mixed meal was consumed (zero time) following an overnight fast (at least 10h). The increase in liver glycogen peaked 5-6h after the meal, with glycogen increasing from 277 mmol/l immediately before the meal to a high of 438 mmol/litre 6 h after the meal (Hwang et al. 1995; Petersen et al. 1996; Taylor et al. 1996). Liver glycogen declined by 30 mmol/l (to a value of 408 mmol/l) by 7 h after the meal, and returned to resting levels at 15h after the meal (Petersen et al. 1996; Taylor et al. 1996), despite an approximately 50% contribution to hepatic glucose production by gluconeogenesis (Petersen et al. 1996).

Muscle glycogen, measured in the gastrocnemius, reached a peak between 4 and 6 h after a mixed meal. The greatest increase in muscle glycogen concentration was

17 mmol/l at 4.9 h, with a subsequent decline of about 10 mmol/l between 6 and 7 h (Taylor et al. 1993). Blood glucose levels peaked at 144 % resting levels 30 min-1h after the meal, declined to 112% resting values at 2h, and then slowly increased to 120% resting levels over the next 2h (4h after the meal; Taylor et al. 1993, 1996; Hwang et al. 1995). From 4 h to 7 h blood glucose steadily declined to reach 111 % resting levels at 7 h after the meal. The changes in blood glucose and liver and muscle glycogen during the first 7 h after a mixed meal are shown in Fig. 7. In order to compare data from the muscle and liver studies, values are given as a percentage of resting levels with resting levels normalized to 100 %. When viewed in this way the interplay between the three variables can be seen, with blood glucose triggering a global synthesis of glycogen over the first 4–6 h following the meal and then global glycogen utilization occurring from 6–7 h. When a standard 70 kg man is used as a model, it can be assumed that muscle comprises approximately 500 g/kg body mass (35 kg). Liver mass is approximately 1.5 kg (or 21 g/kg total body mass; Petersen et al. 1996). If it is assumed that glycogen increases in the gastrocnemius are representative of the total body musculature, then the relative contributions of liver and muscle to glucose disposal can be estimated. Employing these assumptions, approximately 70% of the glucose consumed in a mixed meal is stored in muscle, and when gluconeogenesis is considered the percentage increases to more than 80%.

In summary, the non-invasive nature of ¹³C NMR now allows the routine study of muscle and liver glycogen. Studies of muscle recovery from exercise have been performed, as well as studies of the effect of a mixed meal on muscle and liver glycogen storage. Since the ¹³C techniques can be combined with other NMR measurements, such as ³¹P and ¹H, the possibility now exists to obtain non-invasively and simultaneously data relating to a number of energy metabolites. With this combined information, metabolic studies that were previously impossible are now accessible in a number of different populations.



Fig. 7. Percentage of the resting concentration for blood glucose (\blacksquare), liver glycogen (\bigcirc), and muscle glycogen (\triangle) over the first 7 h following consumption of a mixed meal (300 g containing (g/kg) 500 carbohydrate, 300 fat, 200 protein). Subject populations were normal healthy male and female, aged 18–40 years, without a family history of diabetes (From Price & Rothman, 1999; with permission.)

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This article, and its precursor, has profited from considering a question raised by Dr Coggan about muscle glycogen turnover. In its present form, it is a modified version of the review by Price & Rothman (1999).

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